openheart Utility of conventional aortic root shot angiography for SAPIEN 3 prosthesis sizing in TAVI: feasibility and inter-reader variability

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ABSTRACT

Background The gold-standard approach to prosthesis sizing before transcatheter aortic valve implantation (TAVI) is multislice computed tomography (MSCT). We aimed to investigate whether conventional aortic root angiography (CA) alone can reliably facilitate valve selection and to describe its inter-reader variability.

Methods Five TAVI specialists (3 interventional cardiologists and 2 cardiac surgeons) independently reviewed preprocedural CAs for 50 patients implanted with the Edwards SAPIEN 3 valve.

Results The prosthesis size selected based on visual CA appraisal matched that based on MSCT in 60% of cases (range: 50%–68%), with undersizing in 11% (4%–33%) and oversizing in 29% (10%–46%; $p=0.187$ for equality of the proportions test). Agreement between CA-based and MSCT-based valve selection was moderate ($K=0.41$; $K_w=0.61$). Reassessment of choice following awareness of the annulus long-axis diameter did not significantly improve this agreement (0.40 and 0.63, respectively), though more undersizing (14%) and less oversizing (25%) occurred. Correct valve selection was more common in interventional cardiologists than cardiac surgeons (66% vs 53%; $p=0.0391$), who made more oversizing errors.

Conclusions There is a modest agreement between CA-based and MSCT-based SAPIEN 3 selection. Although the former should not be performed routinely, it may be informative in settings where MSCT and transoesophageal echocardiography are unavailable.

INTRODUCTION

In patients with aortic stenosis undergoing transcatheter aortic valve implantation (TAVI), erroneous estimation of annulus parameters leading to over/undersizing of the transcatheter heart valve (THV) can result in serious consequences.¹ These include annular rupture,² conduction disorders,³ incomplete prosthesis expansion, prosthesis embolisation⁴ and a greater degree of residual paravalvular leak (PVL).^{5,6} Consequently, accurate preprocedural sizing is crucial.

Key questions

What is already known?

► The gold-standard approach to prosthesis sizing before transcatheter aortic valve implantation (TAVI) is multislice computed tomography (MSCT). Although it is true that MSCT has improved the accuracy of long-axis and short-axis annular diameter estimations, particularly in the case of highly calcified valves, it also exposes the patient to harmful radiation and requires the use of contrast agents, limiting its application in patients with renal comorbidity.

What does this study add?

► We aimed to investigate whether conventional aortic root angiography (CA) alone can reliably facilitate valve selection and to describe its inter-reader variability. We found only moderate agreement between the transcatheter heart valve (THV) selection made based on CA aortic root shot assessment and that made using the gold-standard MSCT approach.

How might this impact on clinical practice?

► CA-based THV selection should not be performed routinely for the purpose of valve sizing in resource-rich settings. However, it may be a reasonable approach in the case that MSCT and transoesophageal echocardiography are unavailable, particularly given that it is already a routine step in the TAVI procedure.

Until 2010, transoesophageal echocardiography (TEE) was the most commonly used imaging modality for THV size selection. However, over time it has been gradually replaced by multislice computed tomography (MSCT).⁷ The latter multiplanar imaging technique is now the gold standard for preprocedural assessment of aortic root anatomy, used to determine the form and dimensions of the annulus, its distance from the coronary ostia, the burden and distribution of calcified residues, and AV cuspidity.^{8,9} Although it is true that MSCT has improved the accuracy of long-axis and short-axis annular diameter

Figure 1 MSCT-based valve sizing approach. Example MSCT-based images from a 81-year-old woman with implantation of a 23-mm SAPIEN three valve. Sagittal (A) and coronal (B) multiplanar reformats displaying short and long annulus diameters, respectively (mean diameter of 23.1 mm [21.9+24.3 mm/2]). The corresponding transverse MPR is shown in (C). MSCT, multislice CT.

estimations,^{8–14} particularly in the case of highly calcified valves,¹⁵ it also exposes the patient to harmful radiation and requires the use of contrast agent, limiting its application in patients with renal comorbidity.^{17 16 17} Furthermore, due to its high cost, MSCT may not be available in low-resource settings. For these reasons, it is useful to assess the utility of alternative imaging techniques for valve sizing in TAVI.

Conventional 2D angiography (CA) of the aortic root is routinely carried out during the TAVI procedure.¹⁸ First proposed as an aid to valve sizing in surgical aortic valve (AV) replacement by Mukharji *et al*,¹⁹ this well-established imaging modality is low cost and requires lower radiation and contrast agent doses compared with MSCT. To the best of our knowledge, THV selection based solely on the appraisal of a CA aortic root shot has not been compared with the gold-standard MSCT-based selection. In the present analysis, we aim to ascertain whether reliable TAVI prosthesis sizing is possible based on such CA appraisal alone and to describe the corresponding inter-reader variability.

METHODS

The present study was a retrospective analysis of patients who underwent TAVI at the Augsburg-Schwaben Heart centre (Augsburg Hospital, Germany) between October 2016 and March 2017. The research was approved by the local ethics committee and conducted in line with the Declaration of Helsinki. Written informed consent was unnecessary as existing anonymised data were used.

Only patients who underwent TAVI with the Edwards SAPIEN 3 THV were included in the study. The presence of a bicuspid AV or AV bioprosthesis resulted in exclusion.

Prior to TAVI, each patient underwent prospective ECG-gated MSCT with a high-pitch spiral acquisition, using a third-generation, dual-source CT scanner (Somatom Force; Siemens Healthcare, Germany). The following settings were applied: 250 ms gantry rotation; 66 ms temporal resolution; 2×196×0.6 collimation; a 120 kV tube voltage; and a 350–500 mA tube current. Scan direction was craniocaudal, extending from above the

aortic arch to below the hip. Image acquisition was optimised for the left main coronary artery at 60% of the R–R interval. Contrast agent transit time was measured using the test bolus technique (10 mL of contrast agent followed by a 50 mL saline flush, both administered at a flow rate of 5 mL/s). For MSCT angiography, 50 mL of contrast agent (350 mg iodine/mL; Imeron, Bracco) were injected into an antecubital vein at a flow rate of 5 mL/s, followed by a 60 mL flush consisting of 80% saline and 20% contrast agent. Images were reconstructed using i26f kernel, with a slice thickness of 0.75 mm and an increment of 0.5 mm.

For precise determination of the aortic annulus plane, the lowest insertion points of the right, non-coronary and left aortic cusp were aligned by stepwise manipulation of multiplanar reconstructions (figure 1). The resulting scan was used to calculate aortic annulus parameters and to determine the most appropriate THV size. MSCT image analysis was performed by a cardiologist with several years of cardiac CT experience (level 3) using Agfa Impax software.

Conventional root shot angiography (CA) using the Artis zee system (Siemens Healthcare, Germany) was also performed in each patient prior to THV implantation. This examination included an aortic root shot angiogram (10° left anterior oblique, 10° cranial view) obtained using 10 mL of contrast agent (Iomeprol 350 mg/mL; Imeron 350, Bracco) injected into the right aortic cusp via a 5F curved pigtail catheter. Precise determination of the perpendicular annulus plane was achieved according to the ‘follow the right cusp’ rule.²⁰

After TAVI completion, all preprocedural CA aortic root shots were retrospectively reviewed by five experienced readers (two cardiac surgeons (R1 and R2) and three interventional cardiologists (R3–R5)). Each reader independently estimated the appropriate SAPIEN 3 valve size (20, 23, 26 or 29 mm) based on visual CA image appraisal alone (figure 2A,C). Subsequently, the long-axis diameter of the elliptically shaped AV annulus (‘annular long-axis diameter’) was measured from hinge point to hinge point of the AV cusps (figure 2B,D) and each reader reassessed their selection based on this additional information.

TAVI was performed in the catheterisation laboratory by the resident Heart Team at our institution, consisting of interventional cardiologists and cardiac surgeons. In all patients, the procedure was carried out under conscious sedation with balloon aortic valvuloplasty predilation. Balloon postdilation was performed in the case of treatable residual PVL. At least one additional aortogram was acquired after prosthesis implantation.

Categorical data are presented as absolute values and proportions. Inter-reader agreement was assessed using Cohen’s kappa coefficient, expressed as both unweighted kappa (K) and weighted kappa (Kw), the latter of which also considers the magnitude of the deviation. A Hotelling’s T square test was used to determine the statistical significance of agreements over all raters.

Figure 2 CA-based valve sizing approach. Example of conventional root shot angiography images for a visual appraisal (A and C), with subsequent measurement of the long-axis diameter of the aortic valve annulus (distance from hinge point to hinge point of the AV cusps; shown by a white arrow in (B and D)). Upper panel: an 85-year-old woman with an MSCT-based mean AV diameter of 22.3 mm and implantation of a 23-mm SAPIEN three valve. Lower panel: an 86-year-old man with an MSCT-based mean diameter of 28.5 mm and implantation of a 29-mm SAPIEN three valve. AV, aortic valve; CA, conventional aortic root angiography; MSCT, multislice CT.

Figure 3 Agreement between CA-based and MSCT-based valve size selection when annular long-axis diameter is unknown (A) or known (B). (A) $K=0.41$, $Kw=0.61$. (B) $K=0.40$, $Kw=0.63$. $p=0.951$ for the comparison between (A) K and (B) K ; $p=0.743$ for the comparison between (A) Kw and (B) Kw . CA, conventional aortic root angiography; K , kappa; Kw , weighted kappa; MSCT, multislice CT.

Any difference in the rate of correct valve sizing between physicians was identified using a test for equality of proportions. All statistical analyses were performed using R V.3.4.2, with a p -value of <0.05 considered significant.

RESULTS

In total, 50 TAVI patients met the study criteria and had both an MSCT and CA aortic root shot available for evaluation. MSCT assessment prior to TAVI resulted in the implantation of a 20-mm valve in 1 patient (2%), a 23-mm valve in 23 patients (46%), a 26-mm valve in 16 patients (32%) and a 29-mm valve in 10 patients (20%).

The agreement between visual CA-based valve selection (without knowledge of the annular long-axis diameter) and MSCT-based valve selection was moderate ($K=0.41$; $Kw=0.61$) (figure 3A). On average, valve selection based on the two imaging methods matched in 60% of cases, with CA appraisal resulting in relative undersizing in 11% and oversizing in 29% of cases; however, these proportions varied substantially across individual readers (range: 50%–68%, 4%–22% and 10%–46%, respectively) (figure 4A). Using the CA-based approach, R4 and R5 demonstrated the highest degree of agreement with MSCT-determined valve sizes, followed by R3, R2 and R1 ($K=0.52$, 0.51 , 0.42 and 0.31 , respectively), with a test for equality of proportions resulting in a non-significant p -value of 0.37 (table 1A). In all cases, Kw was higher than K , with the same trend seen across raters ($Kw=0.73$, 0.73 , 0.63 , 0.50 and 0.47 , respectively; $p=0.15$). An inter-rater matrix comparison of K and Kw revealed that there were no statistically significant differences (table 2).

Overall, knowledge of the annular long-axis diameter did not result in a significantly greater agreement between CA-based and MSCT-based valve size selection ($K=0.40$ vs 0.41 , $p=0.951$; $Kw=0.63$ vs 0.61 , $p=0.753$) (figure 3B). Accordingly, there was very little change in the rate of correct valve sizing (mean: 61% vs 60%; $p=0.86$), though more undersizing (mean: 14% vs 11%; $p=0.35$) and less oversizing (mean: 25% vs 28%; $p=0.36$) occurred (figure 4B).

Awareness of the annular long-axis diameter resulted in an increase in K for two readers (R5: 0.52 – 0.56 and R1: 0.28 – 0.32) and a decrease for the other three (R4: 0.51 – 0.48 ; R3: 0.42 – 0.39 ; and R2: 0.31 – 0.28) (table 1). A test for equality of proportions resulted in a non-significant p -value of 0.214 . Kw was again greater than K in all readers, being highest for R5, followed by R4, R3, R1 and R2 (0.77 , 0.74 , 0.62 , 0.54 and 0.47 , respectively).

Overall, the proportion of correctly sized valves was higher when the CA aortic root shot was read by interventional cardiologists compared with cardiac surgeons, regardless of whether annular long-axis diameter was known (66% vs 53%; $p=0.0391$) or unknown (66% vs 52%; $p=0.0177$) (figure 5). Both cardiac surgeons (R1 and R2) were more accurate than their interventional cardiologist counterparts (R3, R4 and R5) when visually judging the need for larger valve sizes, whereas the inverse was true

Figure 4 Proportion of correctly sized/undersized/oversized valves based on CA appraisal without (A) and with (B) awareness of the annular long-axis diameter. 'Correct' valve size is defined as that selected based on preprocedural MSCT. CA, conventional aortic root angiography; R, reader; MSCT, multislice CT; R, reader.

for intermediate-sized valves (table 1A). Additionally, cardiac surgeons less commonly made undersizing errors based on visual CA appraisal, but more commonly made oversizing errors (figure 4A). However, these unbalances became notably less pronounced when the annular long-axis diameter was known (table 1B).

DISCUSSION

The present analysis suggests that CA aortic root shot appraisal results in only modestly accurate prosthesis sizing, as compared with the gold-standard MSCT reference size. Furthermore, CA-based quantification of the annular long-axis diameter did not improve the overall accuracy of valve size selection. As such, CA-based THV sizing should not routinely replace its MSCT-based counterpart. Inter-reader variability was modest, with the interventional cardiologists in our small study generally making more appropriate selections than the cardiac surgeons.

On average, 60% of valves were correctly sized based on the CA aortic root shot, with the fair-to-moderate agreement between CA-guided and MSCT-guided selections.²¹ Although this does not seem to be particularly promising at first glance, it is also important to consider the degree of inaccuracy, with severe over/undersizing resulting in a greater likelihood of complications.²² When the magnitude of each discrepancy was taken into account by K weighting, the moderate-to-substantial agreement was achieved,²¹ suggesting that inaccuracies were largely small. This is further demonstrated by the fact that only 3% of CA-guided valve selections were ≥ 1 size away from their MSCT-guided counterparts. Furthermore, the majority of inaccuracies led to oversizing rather than undersizing errors. This is significant given that moderate oversizing (5%–15% for the SAPIEN 3) has been shown to be protective against postprocedural PVL,²³ whereas undersizing has no clinical utility and results in incomplete apposition to the native aortic annulus.²⁴ In addition, several common oversizing-related complications, such as conduction abnormalities, do not necessarily translate into poorer outcomes,^{25 26} whereas PVL, the most common undersizing-related complication, has been highlighted as an independent risk factor for postprocedural mortality.²⁴ Nevertheless, the advantage of slight oversizing was likely already accounted for in MSCT-based valve selection, meaning that the oversizing observed with CA-based valve selection would be more severe than it first appears. This is concerning, given that severe oversizing of balloon-expandable valves has been associated with a higher risk of aortic root rupture,² a rare (0.5%–1%) but often fatal TAVI complication.²⁷

Although the above-mentioned findings suggest that CA-based THV sizing is not an appropriate substitute for the MSCT gold standard in routine clinical practise, they demonstrate it to provide a reasonable approximation of size requirements, with only a small, non-significant degree of inter-rater variation. As such, it may be useful to guide valve selection in low-resource settings where access to MSCT or TEE technology is limited. Furthermore, given that only a fraction of the contrast agent used for MSCT was required for CA, the latter approach may be an interesting alternative for patients at high risk of contrast-induced nephropathy.²⁸ As always, a balance must be struck between the risks and benefits of each technique.

In general, knowledge of the annular long-axis diameter did not result in a significantly greater agreement between CA-based and MSCT-based valve size selection. Accordingly, there was very little change in the rate of correct valve sizing, though a general trend towards more undersizing and less oversizing emerged. This effect is likely related to the elliptical conformation of the AV annulus. Although MSCT allows calculation of a mean annulus diameter based on measurements of both the short and long axes, with motion-induced artefacts circumvented through gated imaging,²⁹ 2D CA provides data only for the annular long-axis, which must then

Table 1 Number of correct reader assessments when the annular long-axis diameter is unknown (A) and known (B)

	Cardiac surgeons		Interventional cardiologists		
	R1	R2	R3	R4	R5
(A) Unaware of annular long-axis diameter					
20 mm (n/N(%))	0/1(0)	0/1(0)	0/1(0)	0/1(0)	0/1(0)
23 mm (n/N(%))	8/23(35)	7/23(30)	14/23(61)	15/23(65)	18/23(78)
26 mm (n/N(%))	9/16(56)	10/16(63)	11/16(69)	13/16(81)	10/16(63)
29 mm (n/N(%))	8/10(80)	9/10(90)	6/10(60)	6/10(60)	6/10(60)
K (95% CI)	0.28 (0.10 to 0.47)	0.31 (0.13 to 0.50)	0.42 (0.22 to 0.62)	0.51 (0.32 to 0.70)	0.52 (0.33 to 0.70)
Kw (95% CI)	0.47 (0.28 to 0.66)	0.50 (0.32 to 0.68)	0.63 (0.46 to 0.80)	0.73 (0.60 to 0.85)	0.73 (0.60 to 0.86)
(B) Aware of annular long-axis diameter					
20 mm (n/N(%))	0/1(0)	0/1(0)	0/1(0)	0/1(0)	0/1(0)
23 mm (n/N(%))	10/23(43)	10/23(43)	14/23(61)	12/23(52)	20/23(87)
26 mm (n/N(%))	10/16(63)	9/16(56)	10/16(63)	13/16(81)	10/16(63)
29 mm (n/N(%))	7/10(70)	6/10(60)	6/10(60)	7/10(70)	6/10(60)
K (95% CI)	0.32 (0.12 to 0.52)	0.28 (0.08 to 0.48)	0.39 (0.18 to 0.59)	0.48 (0.29 to 0.66)	0.56 (0.37 to 0.75)
Kw (95% CI)	0.54 (0.35 to 0.73)	0.47 (0.27 to 0.66)	0.62 (0.45 to 0.79)	0.74 (0.63 to 0.84)	0.77 (0.66 to 0.88)

K, kappa; Kw, weighted kappa.

be used to approximate the overall annulus diameter, with no compensation for movement. The present data suggest that, on receipt of the long-axis measurements, physicians may tend towards underestimation of the short-axis diameter and selected a smaller THV to compensate. Had this approach been used for valve selection in real life, the result would likely have been greater PVL, poorer transvalvular gradients and less scope for functional improvement.^{5,6} Physician perception seems also to play a role, with the accuracy of two readers improving and that of three readers declining when long-axis data were made available; however, these changes were small. Thus, it may be concluded that the measurement of the aortic annulus long-axis diameter provides a little-to-no clinical advantage in CA-based THV sizing and would prolong interventional times.

Overall, the proportion of correctly sized valves was higher when the CA was read by interventional cardiologists than by cardiac surgeons, regardless of whether the

annular long-axis diameter was known or unknown. This highlights the importance of exploiting the particular expertise and specialty of certain Heart Team members in TAVI, with interventional cardiologists typically having more experience in the appraisal of angiography images.³⁰ Indeed, cardiac surgeons often play a more supportive role in contemporary TAVI at well-established institutions, stepping in the case of procedural complications.³¹ However, based on visual CA appraisal alone, both cardiac surgeons in the present study were more accurate than their interventional cardiologist counterparts in judging the need for larger valve sizes, less frequently making undersizing errors. In contrast, oversizing errors were less commonly made by interventional cardiologists. This highlights the value of the guideline-recommended multidisciplinary Heart Team in TAVI⁸; indeed, it would be interesting to explore whether a collaborative effort towards CA-based valve sizing involving multiple members of the Heart Team would improve the accuracy of valve selection.

Table 2 K comparison using z-test*

		Cardiac surgeons		Interventional cardiologists		
		R1	R2	R3	R4	R5
Cardiac surgeons	R1	–	0.825†	0.313‡	0.093‡	0.078‡
	R2	0.831†	–	0.425‡	0.143‡	0.123‡
Interventional cardiologists	R3	0.243†	0.336†	–	0.531‡	0.491‡
	R4	0.061†	0.096†	0.510†	–	0.960‡
	R5	0.053†	0.086†	0.489†	0.984†	–

*For valve selection based on CA aortic root shot appraisal without knowledge of the annular long-axis diameter.

†Weighted kappa; p-values based on z-test.

‡Unweighted kappa.

CA, conventional root shot angiography; K, kappa.

Figure 5 Comparison of the accuracy of CA-based valve selection between cardiac surgeons and interventional cardiologists with and without awareness of the annular long-axis diameter. CA, conventional aortic root angiography.

The principal limitation of the present study was the small number of readers included, becoming even more relevant when comparing the different types of cardiac specialists. Larger-scale studies would be informative. Furthermore, all readers are current practitioners at the same TAVI-proficient site, meaning that the agreement between them may be higher due to the workplace and geographical influences. As such, the present findings cannot be generalised to other institutions and cardiologists with different levels of TAVI experience. The use of one model of THV, the balloon-expandable SAPIEN 3, also limits the generalisation of results to patients undergoing TAVI with other valve types, particularly self-expanding prostheses. Finally, the assumption that CA-based valve selection was accurate when it matched that indicated by MSCT-based sizing may be misplaced, given that sizing errors are still possible even when using the gold-standard approach. Unfortunately, data on real-world valve undersizing/oversizing at implantation were not available to corroborate MSCT-based selection in the present study.

CONCLUSIONS

There is an only moderate agreement between the THV selection made based on CA aortic root shot assessment and that made using the gold-standard MSCT approach. As such, CA should not be routinely used for the purpose of valve sizing in resource-rich settings. Nevertheless, it may be a reasonable approach in the case that MSCT or TEE is unavailable, particularly given that it is already a routine step in the TAVI procedure. In the case that the CA-based approach is used, the judgement of an interventional cardiologist may be particularly useful for maximising accuracy, whereas the supplementary view of a cardiac surgeon may help to minimise undersizing. However, any time CA-based valve selection is used, balloon sizing prior to implantation is mandatory

to further improve accuracy. Further studies in a larger sample and range of readers would be informative.

Contributors LG and CT: contributed to conception and design of this work. LG, SK, FO, TM-H, WvS and CT: collected the data. BU: designed the statistical approach, analysis and interpretation. PB: outlined the first version of the manuscript, which all other authors revised for important intellectual content. All authors approved the final version of the manuscript to be submitted.

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Correction: *Utility of conventional aortic root shot angiography for SAPIEN 3 prosthesis sizing in TAVI: feasibility and inter-reader variability*

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